Bringing the Hospital to the Patient: Advances in Implantable Nano Sensors

PRESENTED BY: Thomas J. Webster, Ph.D.

Professor of Chemical Engineering, Northeastern University

MODERATED BY:

Steve Redifer

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info@hdiac.org https://www.hdiac.org

Life Expectancy in the U.S.

The Subscribe Economist Not great, again Life expectancy in America has declined for two years in a row Wrong turn Average life expectancy at birth, years That's not really meant to happen in developed countries Japan Print edition | United States > France Jan 4th 2018 United States



25 Years Ago We Turned to Nanomedicine for Some Answers

Nanotechnology: The use of materials whose components exhibit significantly changed properties by gaining control of structures at the atomic, molecular, and supramolecular levels.

Nanomedicine: Applications of nanotechnology in medicine.







Nanostructured Surfaces Improving Health Now



Vascular Endothelialization





Orthopedic Soft Tissue

Helping Amputees



Sketch map of anodization system

PROCEDURES:

<u>Pretreatment</u>: chemical polishing using HF/HNO₃ mixture

Anodization: 0.5 or 1.5%HF

Voltage: 20V

<u>Time</u>: 20 min

Rinse and dry

<u>Clean</u>: acetone and ethanol

Sterilize

Anodized Ti Nanotubular Screws for Osseointegrated Amputee Devices



Closed Wound with No Infection Surrounding Nanotextured Screws Only

Day 14

Day 21

Day 28

Open wound

Anodized nanostructured screws decrease infection, promote skin closure, and increase bone growth



(a) conventional pin



(b) nanorough pin



(c) nanotubular pin

The Emergence of Antibiotic Resistant Bacteria



Colistin-resistant Escherichia coil (E.coil)



Methicillin-resistant Staphylococcus aureus (MRSA)

Bacterial antibiotic resistance causes

- More than 2 million cases of illness and 23 thousand deaths annually (in the U.S. only)
- In 2050, about 10 million deaths and will cost 100 trillion
 USD annually



https://www.cdc.gov/drugresistance/;

https://amr-review.org/Publications.html

THE PROBLEM. ANTIMICROBIAL RESISTANCE TO ANTIBIOTICS (AMR)

What does the future looks like?



So why do nanostructured surfaces *reduce* infection and *increase* tissue growth without drugs ???

Nanostructures in Nature

It has been found that the nanopillars on cicada wings are inherently antibacterial, irrespective of surface chemistry.

• Results show that the cicada wing surface appears to be bactericidal to *Pseudomonas aeruginosa*.



The nanopillar structures of the wing surface are spaced 170nm apart from center to center. Each pillar is ~200nm tall, with a conical shape and a spherical cap 60nm in diameter.

Pogodin et al. Biophysical model of bacterial cell interactions with nanopatterned cicada wing surfaces. Biophys. J. 2013, 104, 835-840.

Possible Reason: Biophysical model





Biophysical model of bacterial cell interactions with nanopillars

<u>Mechanism</u>: As the bacteria try to attach onto the nanopillar structures, the cell membrane stretches in the regions suspended between the pillars. If the degree of stretching is sufficient, this may lead to no attachment or cell rupture.

Pogodin at al. Biophysical model of bacterial cell interactions with nanopatterned cicada wing surfaces. Biophysical Journal, Volume 104, pp. 835-840, 2013.

<u>Possible Reason</u>: Unique Properties of Nano-structured Medical Devices



T. J. Webster, <u>Advances in Chemical Engineering Vol. 27</u>, 125-166, 2001.

Compared to today's implant materials, nano-structured materials possess enhanced:

- surface area,
- radio-opacity,
- catalytic,
- optical,
- mechanical,
- electrical, and
- <u>surface</u>

properties that may improve existing biomedical implant applications.

The Cellular Micro and Nano-environment

Surface micro- and nano-scale topography, grain structure, chemistry, and substrate stiffness modulate cellular functions at the cell-substrate interface¹⁻⁶



 Webster, T. J. et al., Biomaterials 21, 1803–1810 (2000).
 Nikkhah, M. et al., Biomaterials 33, 5230–5246 (2012).
 Bagherifard, S. et al., ACS Appl. Mater Interfaces 6, 7963–7985 (2014).
 Guvendiren, M., Burdick, J. A., Nat. Commun. 3, 792 (2012).
 Dolatshahi-Pirouz, A. et al., ACS Nano 4, 2874– 2882 (2010).
 Dolatshahi-Pirouz, A. et al., J. Funct. Biomater. 2 88–106 (2011).

Predicting Optimal Surface Roughness

<u>Step 1</u>: Obtain data for the surface tension of at least three liquids.

Solvents	Surface Tension (mN/m)			
	γ	Υp	Yd	
DI Water	72.8	46.4	26.4	
Ethylene Glycol	47.7	21.3	26.4	
Glycerol	63.4	26.4	37	

<u>Step 2</u>: Obtain contact angle measurements.

Contact Angle (θ)							
		Square Lattice	Hive™ Lattice				
S(1)	DI Water	91.0°	72.6°				
S(2)	Ethylene Glycol	46.0°	48.9°				
S(3)	Glycerol	94.4°	80.5°				
Wenzel-Corrected Contact Angle (θ_w)							
		Square Lattice	Hive [™] Lattice				
S(1)	DI Water	91.0°	69.7°				
S(2)	Ethylene Glycol	45.1°	40.4°				
S(3)	Glycerol	94.5°	79.0°				

<u>Step 3</u>: Apply Owens/Wendt theory for surface energy values.

$$\frac{\sigma_L(\cos\theta + 1)}{2(\sigma_L^D)^{1/2}} = (\sigma_S^P)^{1/2} \frac{\sigma_L^{P^{1/2}}}{\sigma_L^{D^{1/2}}} + (\sigma_S^D)^{1/2}$$

 σ_L^D = dispersive component of the surface tension of the wetting liquid

 σ_{L}^{P} = polar component of the surface tension of the wetting liquid

 σ_{S}^{D} = dispersive component of the surface energy of the solid

 $\sigma_{S}^{P} = polar \ component \ of \ the \ surface \ energy \ of \ the \ solid$

 $https://www.kruss-scientific.com/fileadmin/user_upload/website/literature/kruss-ar213-en.pdf$

Predicting Optimal Surface Roughness

Step 4: Apply Khang Equation

 $E_s(r_{eff}) = E_{0,s} + \rho \times r_{eff}$



Substrates	Surface Energy (mN/m)			Root-Mean- Square
(Ti6-Al4-V)	γ	γ^p	γ ^d	Roughness, R _q (nm)
Square Lattice	25.4	3.4	22.0	6.08
Hive [™] Lattice	35.7	30.2	5.5	38.5

Step 5: Estimate optimal surface roughness

The optimal Ti surface energy for restricting bacterial biofilm attachment to an implant is **42.5 mN/m**.

When $\rho = 0.3182$ and $E_{0,s} = 23.485$

 $r_{optimal} = 60.5 \text{ nm}$

Khang D, Kim SY, Liu-Snyder P, Palmore GTR, Durbin SM, Webster TJ. Enhanced fibronectin adsorption on carbon nanotube/poly(carbonate) urethane: Independent role of surface nano-roughness and associated surface energy. Biomaterials. 2007;28:4756–68.

Nanoroughness on 3D Printed Spinal Implants (Hive-3)



This surface matches our predicted roughness to decrease infection and promote bone growth

Analyses performed on Hive[™]-1 & Hive[™]-3 samples, square lattice face.

AFM

Hive-3

CONTACT ANGLE



Instrument: Parks Scientific XE-7 AFM XEI Software

Instrument: Phoenix 150 Contact Angle Analyzer ImageJ Software

Ysv



Improved Calcium Deposition on 3D Printed Nano Surface

Calcium Deposition Data – Abcam Calcium Assay Kit



Our prediction works to develop implants that can decrease infection and improve bone growth <u>without</u> drugs

Mineralization assay results are shown, which indicate the capacity for Hive- 3^{TM} implants to promote calcium deposition, and, consequently, osteointegration and growth over 14 and 21 days. Data represents the mean \pm SD: N=9; *p ≤ 0.05 .

Implantable Nanosensors

<u>Current Sensors Used in Medicine</u>: Not at all Like our <u>Immune System</u>





But is this how our body senses events ?



Our body senses "cellular functions"

Implantable Nanosensors: Hip



Real-time Detection of Proteins/Cells/Tissue using Sensors and Releasing Drugs from a PLGA/Polypyrrole Coating

On-going issues with implantable sensors:

- Validation
- Data storage
- Data security

Implantable Nano Sensors

On the Forefront of In-Body Communication and Biosensing on the Nanoscale

Ortho-tag's technologies enable and enhance wireless in body communication, data exchange

Ortho-tag's technologies enable and enhance wireless in-body communication, data exchange and storage, and the nanodiagnostic functionality of smart medical implants, providing a versatile, in vivo platform that connects digital health applications and sensors with the human body. Wand to collect information and stimulate implant

But does this translate in vivo ??

- Implanted square titanium-based sensors into rat calvaria
- Some samples, forced an infection via pre-seeding 10⁵ Staph. epi (and other bacteria in separate experiments) CFU per implant
- Determine bacteria presence, macrophage presence, and bone growth via characteristic cyclic voltammograms
- Assessed tissue growth up to 3 months

Characteristic CVs:

Proving We Transitioned a Hip Implant into a Sensor



<u>Characteristic CVs</u>: Showing Increased Bone Growth With Time



Potential (mV) vs. Ag/AgCl (Scan rate = 300 mV/s)

<u>Reversal of Infection to Increased Bone</u> <u>**Growth: 7 Days Post Implantation**</u>

Push-Out Strength: 0.11MPa

<u>Yellow</u>:

Stain for bacteria



Pre-seeded with *Staph epi* Plain Ti

Similar for *Pseudomonas*, MRSA, and *E. coli* Pre-seeded with *Staph epi* Release of gentimicin and BMP-7 after 1 day Our sensor

0.71 MPa



Similar results for bone cancer and inflammation

Purple: Stain for bone growth

CV of Bacteria Before/After Application of Antibiotic



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Another Example.....

Ever Heard of 4D Printing ????



Matrix Which Can Change Shape On-Demand



4D Printing Implantable Sensors



Another Example.....

Next Generation of Sensors that Could be used in Medicine

Synthetic Cell Sensor:

Need energy source

Need flexible biocompatible materials



Need processing capability

Need responding capability to aid immune cells

Need adaptability

Synthetic nano cells can survey the body for disease, cell mutations, altered immune system, and more to treat such problems immediately.

Next Generation of Sensors that Could be used in Medicine

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Synthetic Immune Nanoparticles



Scale Bars = 100nm

Geilich BM, et. al. Nanoscale. 7 (2015) 3511-3519

And remember...





How many sensors do we have in both ?

VS.





Thank You Again ! <u>E-mail for any questions/collaborations/comments</u>: th.webster@neu.edu

